

A Cost-Effective Hybrid Capacitive-Camera Eye Tracker for Diagnosing Neurodegenerative Diseases

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Introduction

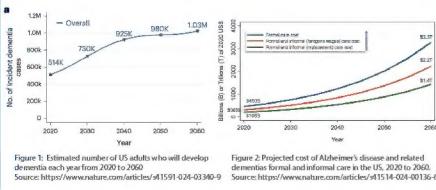


Figure 2: Projected cost of Alzheimer's disease and related dementias formal and informal care in the US, 2010 to 2060. Source: <https://www.ncbi.nlm.nih.gov/pmc/articles/PMC3705110/>

- Neurological conditions can greatly affect a patient's quality of life and pose significant challenges for healthcare systems
- Early diagnosis** can lead to more effective treatments and better results for patients
- Existing screening tests suffer from biases that prevent objective measurements of the patient's cognitive performance
- Eye tracking is a technology that has the potential to offer non-invasive objective measurements of a patient's neurological health through **analysis of eye movements**.
- Most eye tracking devices are video-based, which means that they use cameras to record eye movements. However, to record high-speed eye movements, cameras are not practical, as high-speed cameras are **very costly and inaccessible**.

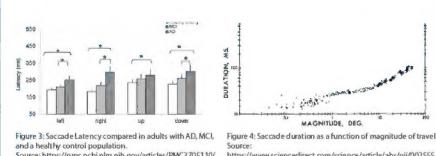
Existing Solutions

	60fps Camera Eye Tracker	1000fps Camera Eye Tracker	1000Hz Capacitive-Camera Eye Tracker
Cost	\$650	\$1000	\$80
Refresh Rate	60Hz	1000fps	1000Hz
Precision	>0.1 degrees	<0.1 degrees	<0.1 degrees

Table 1: Comparison of different eye tracking techniques. Prices estimated from cost of components only.

- For clinical use, the eye tracking device must meet the **required** specifications to accurately track eye movements. These specifications are at least 0.1 degrees of precision and a 1000Hz refresh rate.
- Camera-based eye trackers that use consumer grade cameras are affordable, but cannot meet the required refresh rate.
- Eye trackers that used specialized high speed cameras can meet the required refresh rate, but are significantly more expensive, with the cheapest devices costing over a **\$1000**.
- The hybrid device designed in this study meets the required specifications while only costing **\$80** in components. The cost is much less due to the fusion of a cheap camera-based eye tracker with capacitive sensors that can provide high refresh rates.

Objectives



- 1000Hz refresh rate:** Saccades, which are rapid darting movements of the eye, need to be accurately recorded to gain insights into a person's neurological health. The smallest saccades only last for 25ms, so a 1kHz refresh rate is needed to accurately record their properties.
- 0.1 degrees of precision:** The smallest saccades induce 1 degree of eye rotation, so 0.1 degrees of precision is required to accurately track saccadic motion.
- Less than \$100 in cost:** Eye tracking technology is most needed in communities that don't have access to medical professionals and brain imaging machines, so to maximize accessibility, cost must be kept at a minimum.

Proposal

- The study aims to develop a **hybrid capacitive-camera eye tracker** that meets the performance specifications required for clinical use as a tool to diagnose neurodegenerative disease.
- The proposed device will combine data from a low cost camera recording at 30fps with capacitive sensors that record at 1000hz.
- A **hybrid algorithm** will be developed to combine both data streams while compensating for drifts in the reading or occlusions.
- By combining the spatial resolution of a low-cost camera with the temporal resolution of capacitive sensors, the hybrid device will **approximate the same eye tracking performance** as a regular high speed camera, but at a lower cost.

Methodology

FEM Simulation

- To simulate the precision of the capacitance sensing system, a **finite element method** (FEM) electromagnetic field simulation was conducted.
- The eyeball was modeled as a sphere with a radius of 12mm and the sensor as a square with a side length of 20mm.
- A 12.88ff-change was simulated, correlating to a precision of **0.93 degrees**.

Figure 4: Model of the simulation setup coated in Ansys Maxwell

Figure 5: Stimulated capacitance as a function of eye position. Figure created using Excel from data collected using Ansys Maxwell

Figure 6: SEM image of the surface of laser-induced graphene

Source: <https://www.ncbi.nlm.nih.gov/pmc/articles/PMC3705110/>

Sensor Fabrication

- Laser-Induced Graphene (LIG)** was chosen to create sensitive capacitive sensors because of its high electrical conductivity and surface area
- Polyimide film was heated up using a CO₂ laser to create the graphene sensor.



Figure 7: SEM image of the surface of laser-induced graphene

Source: <https://www.ncbi.nlm.nih.gov/pmc/articles/PMC3705110/>

Figure 8: Photo of the polyimide film being treated using a desktop laser engine

Results

Specification	Horizontal (degrees)	Vertical (degrees)
Accuracy	0.5439 (0.2940)	0.6670 (0.4673)
Precision (RMS)	0.0812 (0.0345)	0.0889 (0.0395)

Table 2: Eye tracker specifications, where accuracy and precision are given in degrees, and the refresh rate is measured in hertz. The numbers in parentheses are the standard deviations

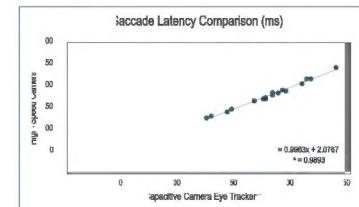


Figure 10: Example images taken from the device's camera. Left shows an image with a high confidence score of 1.0. Right shows an image with a low confidence score of 0.7.

Pupil Identification

- Figure 9: Steps of the PuRe algorithm (left to right): grayscale, crop eye region, edge detection, confidence score. It shows 4 segments, including a combined segment. Images taken from Cunliffe et al., 2018.
- To track the eye movements in the camera frame, the PuRe pupil identification algorithm was implemented.
- The algorithm uses an **edge selection algorithm** to identify the elliptical pupil in the camera frame. The algorithm also outputs a **confidence score** for the identified pupil.

Figure 10: Example images taken from the device's camera. Left shows an image with a high confidence score of 1.0. Right shows an image with a low confidence score of 0.7.

Frame Construction

- The first iteration of the device used a 3D printed pair of glasses as the base of the device. The frame was lightweight and easy to construct, but could not adjust to different face shapes, and could shift around, leading to **inaccurate tracking**.
- The second iteration of the device used the frame of an old VR headset. The frame provided foam padding and an adjustable size, allowing for a tight but comfortable fit on the user's head.
- A single 10ft USB 3.0 cable was used for all data communication, with the camera and arduino microcontroller connected through a USB hub. The capacitive sensor was placed in a plastic enclosure to minimize **parasitic capacitance**.

Figure 11: Second iteration of device frame, using an adjustable head strap



Figure 12: Graphical representation of the hybrid algorithm over the course of 0.7 ms. Top blue bars represent each capacitance measurement. Middle green bars represent each camera frame. Bottom represents the output gaze prediction as a hybrid of the two.

Hybrid Algorithm

- The hybrid algorithm fuses 30hz data from the camera with **1000hz** data from the capacitive sensor to output a single gaze prediction. The algorithm runs once every millisecond and works as follows:
 - If a new camera frame is available and the confidence score is above a set threshold, use only the camera frame to make the gaze prediction.
 - If a new camera frame is not available, take the change in pupil location measured by the capacitive sensors and add it onto the last obtained pupil location from the camera.

$$P(t) = F(t) + C(t) - C(t_0)$$

Figure 11: The equation for the hybrid algorithm, where $P(t)$ is the gaze prediction at any time t , $F(t)$ is the time of the last available camera frame, $F(t_0)$ is the gaze prediction from the last available camera frame, and $C(t) - C(t_0)$ is the change in gaze prediction measured by the capacitance sensor from time t_0 to t .

Software Integration

- Figure 13: Block diagram showing the flow from camera to sensor inputs to the hybrid algorithm.
- Two separate computers were used to implement the hybrid device. An **Arduino microcontroller** was used to read the capacitance measurements from the sensor chip and send the data over serial to an external laptop. The camera directly sent the recorded image frames to the laptop.
- On the laptop, two separate processes were ran at once. One process ran the **pupil identification algorithm**, while the other process ran the **hybrid algorithm**, outputting the final gaze prediction.



Prototype Validation

Research Trial

- To measure the performance of the device, a research trial was conducted with **10 volunteers** (ages 16-60).
- The trial was set up on a table with a monitor for displaying the stimulus.
- The trials began with a calibration screen, and then 3 tests were conducted to measure different eye metrics.

Figure 14: Calibration screen showing a crosshair and a fixation point.

Figure 15: Calibration screen showing a crosshair and a fixation point.

Figure 16: Diagram of the setup for the research trial, including the hybrid device, high-speed camera, and computer monitor.

Figure 17: Eye stimulus screens during the trial.

Figure 18: High speed camera used during the trial (Buster Ace ac640-750um). Zoom lens was used to record only the eye movements. Recorded video at 1000fps over ethernet.

Benchmark Comparison

- During the research trial, a **high speed camera** was also recording the volunteer's eye movements. The high speed camera provided a benchmark to compare to the hybrid device.
- By comparing the recorded eye metrics from both devices, the validity of the hybrid device as a true replacement for high-speed camera eye trackers can be tested.
- The high speed camera was mounted to the table during the trial and recorded at **1000fps**.

Figure 19: High speed camera used during the trial (Buster Ace ac640-750um). Zoom lens was used to record only the eye movements. Recorded video at 1000fps over ethernet.

Data Analysis

Cross-Sensor Calibration

- To allow for merging of the two sensor readings, a calibration procedure was conducted at the beginning of the trial. A **third-order polynomial regression model** was then fitted to establish a transformation function that converts raw capacitive sensor data into pupil coordinates that align with the camera's output.

Confidence-Based Filtering

- The pupil detection algorithm assigns a confidence score between 0.0 and 1.0 to each detected pupil location.
- Calibration points where the confidence score was below 0.95 were **discarded** to prevent inaccurate data from affecting the model.

Performance Specifications

- The difference between the true eye position and measured eye position was used to calculate the error. The error was averaged across all recorded points to find the average accuracy.
- To calculate the precision of the device, the **root mean square** (RMS) of the angular distance between every recorded point during the fixation test was measured.
- For each recorded eye metric, the values were calculated using the technique established by (Pavicic et al., 2017).

Conclusion

Summary of Findings

- By leveraging the **high spatial resolution** of cameras with the **high temporal resolution** of capacitive sensors, the developed hybrid eye tracker provides high speed eye tracking at a lower cost.
- In testing, the device measured eye metrics within 4% of the values recorded by a high speed camera, but with a **92% reduction** in cost.
- Eye trackers have the potential to offer **objective non-invasive measurements** of a patient's neurological health, offering a significant advantage over traditional paper tests that can introduce biases and inconsistencies due to the need for a human examiner. The low cost of the hybrid device improves the accessibility of the technology.

Significance

- The next steps for the device include running **clinical trials**, where patients with neurodegenerative disease are tested using the hybrid device and the results are then compared to traditional cognitive tests.

Future Work